Present and Future Hyperthermia Technology Evolution

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How are we doing?

- Reviewed 29 randomized/Phase III studies
- Reviewed criteria as reported
 - Complete response rates
 - Disease Free Survival
 - Overall survival
 - Toxicity Grade III and IV



Randomized Studies Reviewed

Author	Site	Pat. #
Issels	S Sarcoma	341
Issels (JAMA)	s Sarcoma	341
Zee	cervical	114
Zee	bladder	101
Zee	rectal	143
Jones	breast	109
Vernon	breast	306
Overgaard	melanoma	128
Colombo	bladder	75
Sneed	brain	79
Valdagni	Head/neck	44
Huilgol	Head/neck	56
Harima	cervical	40

Author	Site	Pat. #
Cornett	S Sarcoma	124
Kitamura	esophagus	66
Sugimachi	esophagus	40
Datta	Head/neck	65
Arends	Bladder	190
Perez	local	307
Perez	Local<3cm	
Emami	H&N/Pelv	184
Hua	nasoph	180
Siwinska	cervical	76
Egawa	VariousSuper	92
Sharma	cervical	50
Vasanthan	cervical	110









% Overall Survival 46% with HT vs 38% per Patient (for 2300 Patients)

HT + RT or CT or Both RT or CT or Both





% Disease Free Survival 46% with HT vs 37% per Patient (for 924 Patients)



% Toxicity Grade III and IV 9% with HT vs 5% per Patient (for 1484 Patients)





BSD-500, 915MHz, Eight Outputs 0- 60watts or single 400watt output channel, non-metal temperature probes with No MW artifact or interference, Superficial and interstitial applications, CE Mark



Current microwave systems

ALBA 434MHz, 0-200Watt, Single Channel, Metal Thermocouples with MW artifact and interference. Superficial and intracavity, CE Mark







Microwave Future Thoughts

- Superficial arrays for dynamic control of surface temperature distribution
- Improved water bolus interface options
- Pretreatment planning software tools
- More conformal patient interface
- Greater implementation with Brachytherapy



Greater Clinical Use of Microwave Arrays – 8 Spiral Array Being Updated







Volts



Spiral Arrays of 8, 5 and 3 Spirals For Improved Temperature Uniformity









BSD Spiral Sheet Hyperthermia Applicator 2.5cm Bolus 5mm Plane in Muscle Phantom. Most Uniform Case SAR Normalized to 5mm Plane.





Deep Heating Methods

- RF Capacitive
- RF Phased Array
- HIFU





Oncotherm EHY-2030, 13.56MHz, Protocol 150W Max Power, Generator 600W



Capacitive electrodes have remained basically the same since 1917 in tumor treatments. Similar to modern toasters evolution.



Some Capacitive Electrodes uses cooling water bolus to reduce excess fat heating with cooling depth limited to 1.5cm of fat.



RF Phased Array Methods

- Surround a body portion with an array of RF field antennas
- Use phase and power control to steering deep focal heating location
- E-field is dominantly parallel to the body to reduce fat heating and boost central focus



Sigma30 (MAPA), SigmaEye, Sigma60



AMC-4 system 1987 70MHz 4 RF Channels

AMC-8 system 70MHz 8 RF Channels 2 Rings







ALBA 4D, 70MHz, 4Channels 500w each, Metal thermocouples

Awaiting independent clinical validation of this configuration.

Reliability and clinical utility are yet to be established

1981 four waveguide technology has a new look





Deep Heating Numerical Study

- COMSOL 3D Multiphysics Model
- Homogeneous phantom cylindrical and elliptical saline or muscle dielectric and 2/3rds muscle conductivity with 1cm layer of superficial fat.



Sigma 60-8 dipole array@ **100MHz** using a COMSOL numerical model of a 28cm diameter phantom 74cm long & 48cm long water bolus. This study showed more selective central heating with low fat heating near the bolus outer edges. Maximum SAR is shown in the tissue center.

Axial Slice View

Coronal Slice View



Sigma 60-8 dipole array@ **75MHz** using a COMSOL numerical model of a 28cm diameter phantom 74cm long & 48cm long water bolus. This study showed stable and uniform surface and central heating with and increase of fat heating near bolus outer edges as compared with the heating at the center.



Coronal Slice View



AMC-4 Waveguide array@ **70MHz** using a COMSOL numerical model of a 28cm diameter phantom 74cm long & **40cm** long water bolus. This study showed high superficial fat SAR potential.



Capacitive Electrodes Have No Energy Focus 1917 Technology







Capacitive field divergent current

- If RF currents diverge 1.7 times the electrode diameter at depth, the expanding area at depth is (1.7)² = 2.9 times larger at the phantom center, so the RF current is 1/2.9 times less than under fat.
- SAR= I^2R = (1/2.9)² R= R/8= 1/8th of the muscle surface.
- For heating a central tumor or for a possible non-thermal modulation effect, the RF power must reach the target with an adequate level to be effective.



RF currents from capacitive electrodes will only converge if bone, fat, and air regions divert these currents to concentrate them. The visceral fat distribution is unique to a patient and limits any consistent deep heating results from capacitive electrodes in patients with visceral fat.





There is a limited future for capacitive electrodes in deep heating

- Superficial fat layer absorption
- Field shape is divergent with lack of control
- RF current flow paths are altered by visceral fat
- Not compatible with image guided SAR steering
- Dump and pray for an RF conductive path to reach the tumor



The Future is Phased Arrays For Deep Heating







2017 Munich Installation



Universal System approved for clinical use











2019 New Developments In Process





-Universal Water System Design -Software Controls for Universal Water System -All-In-One Computer/Desktop Console



Pyrexar MEDICAL

New BSD-2000 MR Water System

Major Improvements

- Improved Air Removal and Pressure Monitoring (7)
- Leak Catch Tub and Leak Detection (8)
- On-Board 1 Ton Chilling Unit for Improved Site Flexibility (10)
- Sensor Additions allow for Software Functionality Improvements without updated Hardware:
 - Possibility for automated Fill/Drain Capability
 - Possibility for automated Bolus Air Removal
- Addition of Pedestal LED Flow Indicator
- Addition of System Control Function Buttons on Electrical Box for Quick Troubleshooting
- No Need for Deionizing Filter due to Closed System Architecture – Breathable .3μm Filter Resists Contamination (4)
- 3 Separate Water Level Sensors for Improved Communication to Operator and Smart Controls (5)
- Added Ability to Drain and Refill System from Pedestal
- Adjustable Chilled Water Source Temperature for
 Patient Comfort during Circulation





BSD-2000 Hyperthermia System TEST

Hyperthermia Treatment

Planning

Sensor Setup

Recall

Utilities







Noninvasive brain applicator Hal.o

- Operating frequency: 915 MHz
- Array: 3 rings of 24 antennas (dipole size 9×24 mm)
- Cylindrical frame: 13 cm length, 26 cm dia. (~4cm water bolus)





Making A Difference in Cancer Care Patent pending



Steering with different number of amplifiers



Sim vs Exp MR thermometry after 3min of heating target (0,0,0)

MR thermometry



Heat focus ~25s after power off 4 × 2 × 2 cm³



Sim vs **Exp** MR thermometry: Mechanical steering Phantom shifted vertically 1.5 cm \rightarrow Focus is kept at the applicator center MR thermometry Simulation ΔT (°C) 2.5 $+1.5^{\circ}$ 2 1.5 Phantom 1 -1.5° Water 0.5 $\Delta z_{\text{focus,exp}}$ = 1.5 cm Making A Difference in Cancer Care $\Delta z_{focus,sim}$ = 1.5 cm

Sim vs Exp MR thermometry: Electronic phase steering





New deep heating practices

- Non-centered patient phase steering
- Superficial heating by power control
- Future MR image guided treatment optimization.





Vertical phantom +2cm (0,5) cm focus (0,5)-(0,2)=(0,3)



Centered phantom (0,3) cm focus

Naking A Difference in Cancer



Vertical phantom +2cm (0,-1) cm focus (0,-1)-(0,2)=(0,-3)



Centered phantom (0,-3) cm focus

rexar



Sigma 60 Superficial SAR Prediction at 90MHz by SigmaHyperPlan Using RF Power On Only 1 or 2 Power Channels



Future developments need to understand frequency dependence of field interaction caused by the cell membrane

0.1 to 100MHz RF currents flow	High Microwave Frequency currents
around the cell	pass through the cell >100MHz
Higher	Heat Cell
Membrane	Interior
Voltage	Directly

R. Pethig, Dielectric and Electronic Properties of Biological Materials, John Wiley & Sons, 1979 Making A Difference in Cancer Care



Muscle Tissue Dielectric and Conductivity Due to Cell Membrane Capacitance and Water Resonance



R. Pethig, Dielectric and Electronic Properties of Biological Materials, John Wiley & Sons, 1979



Numerical Advanced Study

- COMSOL 3D Multiphysics Model
- Homogeneous phantom cylindrical and elliptical saline or muscle dielectric and 2/3rds muscle conductivity with 1cm layer of superficial fat.
- More than 300 solutions with different variations evaluated.





Time=300 Multislice: Electromagnetic power loss density (W/m³)







250MHz, Propylene glycol bolus 24 dipoles & channels, muscle phantom, Vol=176cc









175 MHz Axial View, 3D Optimization Central Focus
24 channels and dipoles, 10.6 cm dipoles,
48 cm wide bolus, 60 cm dia. water bolus.
6.9x6.9x13.4cm, Vol.= 334cc





Axial

Sagital

Coronal

175MHz 24 channel System 4cm Steering Muscle Phantom, PG Bolus





175MHz 24 channel System 4cm Steering Muscle Phantom & PG Bolus





140MHz Sigma Eye 24 dipoles & 3 rings, **Water Bolus**, 2/3rd Conductivity Muscle Phantom 13.6x12.3x20.2cm,Vol=1,769cc







250MHz Elliptical SigmaEye, Saline Phantom, Central 3D focus, PG Bolus 4.3x6.2x11.0cm, Vol.= 143cc.



RF vs HIFU Phased Array

	RF Phased Array	HIFU Phased Array
Focus	Large	Small
Focal Steering	Simple	Complex
Air & Bone	Tolerant	Blockage
Large Tumors	Suitable	Limited
Dose Monitoring	Easy	Difficult
SAR Pattern	Uniform	Non-Uniform



Future Clinical Applications

- Proton therapy with HT
- Renewed interest in Brachytherapy +HT
- Immune response with HT
- Brain targeted phased array treatments
- Superficial arrays for more uniform surface heating



Treatment Tools Being Planned

- Brain phased array Hal.o
- Advanced high frequency phased array
- MR guided focused thermal therapy
- Superficial arrays
- Further evolution of current systems
- Advancements in treatment planning

